BIOELECTRONICAL NEURONAL NETWORKS

Towards chemical analysis by coupling neurobiological entities to capacitive or capacitive-optical transducers

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In awe of nature and its marvelous secrets

ABSTRACT

This thesis depicts the development of an **autonomous** *in vitro* recording system for neuronal cell cultures. It is intended to be used in analytical chemistry and sensorics as a transportable system independent from laboratory facilites. As the sensing entity, a neuronal network is cultured in a perfusion chamber mounted on a passive 60-electrodes multimicroelectrode array. The response behavior of that network to analytes will be recorded, amplified, and analyzed mathematically in the sub-millisecond range.

Besides the portrayal of the mechanical and electronical design of a modular, temperature controlled perfusion chamber, of a life-maintaining support system, and of a 60-channel amplifier for signal recording, various secondary problems have been addressed and partly solved in this context. These include post-modification procedures of the recording electrodes with respect to the improvement of their electrical as well as adhesion mediating properties.

Neuronal cultures from embryonic chicken may survive in the **modular, temperature controlled perfusion chamber** for up to three weeks. Their development and differentiation cannot be distinguished from cultures grown on cell culturing trays in CO₂-incubators. Cell survival turned out to be strongly dependent on perfusion parameters. While a constant fast-volume flow (15 μ l/hour, equivalent to approx. 1/5th of the total chamber volume) of fresh medium through the chamber stressed the cultures noticably, timed perfusion of about 30 μ l once or twice a day kept the cultures viable. Longevity was limited rather by mechanical and electronical problems with the perfusion chamber and the controlling unit than by principle faults in the concept.

A **60-channel amplifier** in a sandwich configuration (32 + 28 channels) with very good noise and speed characteristics may amplify neuronal signals by a factor of 990 or 1551, respectively. However, for not yet understood reasons, the offset of that system is pulled to the lower supply potential of -5 V. The amplifier is connected to a high-speed (333 ksamples per second) data acquisition board with a total of 64 A/D-channels. A **signal recording program** in a virtual-instruments programming environment (TestpointTM by Keithley Instruments, Inc.) has been developed.

The electrical behavior of the recording (and stimulation) electrodes with respect to a high capacitance, a high charge delivery capacity, a low impedance, and biocompatibility, has been improved by **electrochemical iridium deposition** (and iridium oxide formation) onto platinum from an aqueous solution of H_2IrCl_6 . It turned out that various iridium layers of different and decreasing stabilities with increasing thicknesses will form on the electrodes. To enhance mechanical stability of those deposits, iridium may be embedded in a polypyrrole matrix. The total impedance could be lowered by almost two orders of magnitude in the low frequency range below 1 kHz with respect to a plain platinum electrode while the increase of electrode capacitance by almost two orders of magnitude did not suffer from the matrix environment.

Neuronal cultures from embryonic chicken may be grown in **serum-free medium** and will survive in some cases for up to 6 months in a standard CO_2 -incubator. Cell development in serum-free medium lags noticably behind that of cells grown in medium that contains 10% (v/v) fetal bovine serum within the first two weeks. However, if the density of seeded cells surpasses a certain threshold (at least complete surface coverage of the substrate), cell networks grown in different media cannot be distinguished thereafter.

New **adhesion strategies** on the base of electroactive phenol and pyrrole derivatives for the selective coverage of electrodes have been developed. Besides mimicking standard laminin related adhesion promoting procedures with the help of a peptide fragment from laminin (*SRARKQAASIKVAVSADR*) that is linked to an electroactive monomer (e.g. 3-hydroxyphenylacetic acid), electropolymers of 2-(3-hydroxyphenyl)-ethanol and of 3-hydroxybenzyl hydrazine have proven to promote cell adhesion (and neuron differentiation) in serum-free medium. Furthermore, it has been observed that laminin or a combination of laminin and polylysine will not promote cell adhesion and neuron differentiation in serum-free culture while they work perfectly well in medium with serum. This finding might hint at an indirect adhesion mechanism of laminin that depends on secondary 'mediating' factors found in the medium, while the adhesion promoting properties of polymeric films mentioned above might be based on a more direct cell-film interaction.

As an alternative to capacitive-electrical electrode arrays with limited areal resolution, especially when studying signal spread, principle characteristics of a new **capacitive optical recording array** based on potential sensitive fluorescent dyes have been investigated. To circumvent common problems with membrane-bound potential sensitive dyes, the dyes will be trapped in a polymeric film on a suitable electrode material instead and thus stay in direct contact with the neurons. It could be shown that this strategy is working in principle by exhibiting voltage dependent fluorescence quenching. However, probably due to polymer thicknesses in the range of micrometers, the potentials necessary for generating noticable signals are still beyond capacitively detectable neuronal signals by almost four orders of magnitude.

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CONSTANTS

Basic constants

$R = N_A \cdot k$	gas constant	8.31441	$J \cdot mol^{-1} \cdot K^{-1}$ $m^2 \cdot kg \cdot s^{-2} \cdot mol^{-1} \cdot K^{-1}$
$F = N_A \cdot e$	F_{ARADAY} constant	96484.56	C·mol ⁻¹ A·s·mol ⁻¹
$N_{\rm A}$	<i>AVOGADRO</i> or <i>LOSCHMIDT</i> constant: # of particles per mol	$6.022045 \cdot 10^{23}$	mol ⁻¹
e	elementary charge: charge of one electron	1.6021892·10 ⁻¹⁹	C A·s ⁻¹
k	BOLTZMANN constant	1.380662.10 ⁻²³	$J \cdot K^{-1}$ m ² ·kg·s ⁻² ·K ⁻¹
Т	Temperature		K 0°C = 273.16 K
h	<i>PLANCK</i> constant	6.62608·10 ⁻³⁴	$J \cdot s$ $m^2 \cdot kg \cdot s^{-1}$
ϵ_0	permittivity of the vacuum	8.854187817·10 ⁻¹²	$F \cdot m^{-1}$ $C \cdot V^{-1} \cdot m^{-1}$ $C^{2} \cdot J^{-1} \cdot m^{-1}$

ABBREVIATIONS

Amino acids

cod	es	amino acid	molecular formula	FW	polarity	pK _a *
G	Gly	glycine	C ₂ H ₅ NO ₂	75.1	+2.4	
A	Ala	alanine	$C_3H_7NO_2$	125.6	+1.9	
V	Val	valine	$C_5H_{11}NO_2$	117.2	+2.0	
L	Leu	leucine	$C_6H_{13}NO_2$	131.2	+2.3	
Ι	Ile	isoleucine	$C_6H_{13}NO_2$	131.2	+2.2	
C	Cys	cysteine	$C_3H_7NO_2S$	121.2	-1.2	8.3
М	Met	methionine	$C_5H_{11}NO_2S$	149.2	-1.5	
F	Phe	phenylalanine	$C_9H_{11}NO_2$	165.2	-0.8	10.1
Y	Tyr	tyrosine	$C_9H_{11}NO_3$	181.2	-6.1	
W	Trp	tryptophane	$C_{11}H_{12}N_2O_2$	204.2	-5.9	
Р	Pro	proline	C ₅ H ₉ NO ₂	115.1	-6.0	
S	Ser	serine	C ₃ H ₇ NO ₃	105.1	-5.1	
Т	Thr	threonine	C ₄ H ₉ NO ₃	119.1	-4.9	
N	Asn/Asx	asparagine	$C_4H_8N_2O_3$	132.1	-9.7	
Q	Gln	glutamine	$C_{5}H_{10}N_{2}O_{3}$	146.1	-9.4	
D	Asp	aspartic acid	$C_6H_{14}N_4O_2$	174.2	-11.0	4.0
Е	Glu/Glx	glutamic acid	C ₅ H ₉ NO ₄	147.1	-10.2	4.3
Н	His	histidine	$C_6H_9N_3O_2$	155.2	-10.3	6.0
K	Lys	lysine	$C_6H_{14}N_2O_2$	146.2	-15.0	10.8
R	Arg	arginine	$C_6H_{14}N_4O_2$	174.2	-20.0	12.5

One-letter code and three-letter notation [KOO 95 · MAL 98]

*Note: The change in free enthalpie ΔG for the transfer of the side-chain from a rather non-polar solvent (ethanol) to a very polar solvent (water) is a measure for polarity of the side-chain. The more negative the value for ΔG the more polar is the side-chain.

Other abbreviations

2(3HPE)	2-(3-hydroxyphenyl)-ethanol	DMAP
3HBA	3-hydroxybenzaldehyde	DMF
3HBH	3-hydroxybenzylhydrazine	Е
3HPA	3-hydroxyphenylacetic acid	EIS
3PPA	3-(pyrrole-1-yl)-propionic acid	EP
a	activity	ES
AC / a.c.	alternating current	F
ACA	ε- a mino c apronic a cid	FET
ADP	adenosine diphosphate	FIA
AIROF	(anodically) a ctivated i ridium o xide f ormation	GB
APS	active pixel sensors (CMOS-based digital camera chip)	HPLC
ATG	β -alanine-tetraethylene glycole-glycine	HTS
ATP	adenosine triphosphate	Hz
ATR-IR	attenuated total reflection infrared (spectroscopy)	Ι
BDNF	brain derived neurotrophic factor	i
С	electrical capacity $[C] = F = C \cdot V^{-1}$	IC
CAM	cell adhesion molecule	ID
CCD	charge coupled device	IHP
CDC	c harge d elivery c apacity $[CDC] = C \cdot cm^{-2}$	IME
CE	counter electrode	IS
CMOS	complementary metal-oxide semiconductor	ISA
CNS	central nervous system	ISFET
CNTF	ciliary neurotrophic factor	ITO
CoA	coenzyme A	J
CV	cyclovoltammetry	1
CVD	chemical vapor deposition	L
d	postnatal day	LAPS
D	constant of diffusion $[D] = cm^2 \cdot s^{-1}$	LSD
Da	\mathbf{Da} lton = MW	М
DC / d.c.	direct current	m
DCC	dicyclohexylcarbodiimide	m (as prefix)
Di I	DilC18(3) or 1,1'-dioctadecyl-3,3,3',3'- tetramethylindocarbocyanine perchlorate	ManLe
dic	days in culture	MB

DMAP	4-dimethylaminopyridine		
DMF	N,N'-dimethylformamide		
E	embryonic day		
EIS	electrochemical impedance spectroscopy		
EP	electroplated		
ES	embryonic stem (cells)		
F	farad $[F] = C \cdot V^{-1} = s \cdot \Omega^{-1}$		
FET	field effect transistor		
FIA	flow injection analyser		
GB	\mathbf{g} iga \mathbf{b} yte = 1 · 10 ⁹ bytes = 8 · 10 ⁹ bits		
GC	gas chromatography		
HPLC	high performance liquid chromatography		
HTS	high throughput screening		
Hz	HERTZ [Hz] = s ⁻¹		
[current [I] = A		
	$\frac{i\pi}{2}$		
	imaginary unit: $i \equiv \sqrt{-1} \equiv e^{-2}$		
IC	integrated circuit		
D	inner diameter		
ΗP	inner <i>HELHOLTZ</i> plane		
ME	interdigitated microstructured electrode		
IS	impedance spectroscopy		
ISA	industrial standard adaptor		
SFET	ion sensitive field effect transistor		
TO	indium-doped tin oxide		
ſ	$JOULE [J] = kg \cdot m^2 \cdot s^{-2}$		
	liter		
L	inductance $[L] = HENRY = V \cdot s \cdot A^{-1}$		
LAPS	light addressable potentiometric sensor		
LSD	lysergic acid diethylamide		
М	molar concentration $[M] = mol \cdot l^{-1}$		
n	meter		
n (as prefix)	milli (10 ⁻³)		
ManLev	N-laevulinic acid-D-mannosamide		
MB	\mathbf{m} ega \mathbf{b} yte = $1 \cdot 10^6$ bytes = $8 \cdot 10^6$ bits		

MEA	micro electrode array	RE	reference electrode
MEM	minimum essential medium	RH 421	potential sensitive dye; N-(4-sulfobutyl)-4-
MMEP	multi micro electrode plate		(4-(4-(dipentylamino)phenyl) butadienyl)pyridinium, inner salt
mol	mole : number of particles in a sample: 1	RIE	reactive ion etching
	particles as there are atoms in exactly	RIFS	reflectometric interference spectroscopy
	12 grams of carbon (^{12}C) .	s	second
MOS	metal oxide semiconductor	S/N	signal-to-noise ratio
MOSFET	metal oxide semiconductor field effect transistor	SCE	saturated calomel electrode ($E^0 = +0.242V$ @ 25°C)
Mr	r elative m olar mass $[Mr] = g \cdot mol^{-1}$	SCIL	save charge injection limit = RCDC
MW (FW)	m olecular weight [MW] = $g \cdot mol^{-1}$	SEM	scanning electron microscopy
n	nano (10^{-9})	SFM	scanning force microscopy
NCAM	neuronal cell adhesion molecule	SFM	serum-free medium
NGF	nerve growth factor	SMD	surface mounted device
NHE	n ormal h ydrogen e lectrode ($E^0 = +0.242V$	SOT23	small outline transistor: a standardized packaging size for CMOS devices
OD	auter diameter	SP	sputtering / sputter deposition
OHP	outer Hei Hoi TZ plane	Т	absolute temperature $[T] = K$, 1 K = 1°C
onamn	operational amplifier	THF	tetrahydrofuran
PC		UV	ultra-violet radiation
PCA	principle component analysis	V	volt $[V] = J \cdot C^{-1} = W \cdot A^{-1} = kg \cdot m^2 \cdot s^{-3} \cdot A^{-1}$
PCR	principle component regression	VD	vapor deposition
	poly D lysine	VIS	visible light
DEA	planar alaatrada array	WE	working electrode
PECVD	plasma enhanced chemical vanor	XPS	X-ray photoelectron spectroscopy
TECVD	deposition	z	valency of an ion
PEG	poly-ethylene glycole	Z _C	ractance of a capacitor
pН	potentia hydrogenii: -log [H ⁺]	Z_L	reactance of an inductance
PNS	peripheral nervous system	$Z_{\rm W}$	WARBURG impedance
PTFE	p oly t etra f luor e thylene (Teflon [™] ,	BAEE	$N\alpha$ -benzoyl-L-arginine ethyl ester
BVD	plasma vanar danasitian	ε _r	relative electrical permittivity = relative dielectric constant
P V D		0	GALVANI potential
ĸ	resistance $[R] = \Omega$	φ	miero (10 ⁻⁶)
RAM	random access memory	μ	
RCDC	reversible charge delivery capacity = RCIL = SCIL	ν ω	$requency [v] = s^{-1}$ angle velocity [w] = s ⁻¹
RCIL	reversible charge injection limit = SCIL = RCDC		